



Data-driven cortical clustering to provide a family of plausible solutions to M/EEG inverse problem

Kostiantyn Maksymenko, Maureen Clerc, Théodore Papadopoulo

► To cite this version:

Kostiantyn Maksymenko, Maureen Clerc, Théodore Papadopoulo. Data-driven cortical clustering to provide a family of plausible solutions to M/EEG inverse problem. iTWIST, Nov 2018, Marseille, France. hal-01946876

HAL Id: hal-01946876

<https://hal.inria.fr/hal-01946876>

Submitted on 6 Dec 2018

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

Data-driven cortical clustering to provide a family of plausible solutions to M/EEG inverse problem

Kostiantyn Maksymenko^{1,2}, Maureen Clerc^{1,2} and Theodore Papadopoulos^{1,2}.

¹University of Côte d’Azur, France. ²INRIA Sophia Antipolis, France.

Abstract— The M/EEG inverse problem is ill-posed. Thus additional hypotheses are needed to constrain the solution space. In this work, we consider that brain activity which generates an M/EEG signal is a connected cortical region. We study the case when only one region is active at once. We show that even in this simple case several configurations can explain the data. As opposed to methods based on convex optimization which are forced to select one possible solution, we propose an approach which is able to find several ”good” candidates - regions which are different in term of their sizes and/or positions but fit the data with similar accuracy.

1 Introduction

Human magneto-/electroencephalographic (M/EEG) [1] source localization aims to reconstruct the current source distribution in the brain from one or more maps of potential differences measured noninvasively from electrodes on the scalp surface (EEG), or maps of magnetic fields measured by magnetometers (MEG). A common approach is to represent the cortex as a finite set of current dipole sources. The M/EEG signal generated by such a source with a unit amplitude is called lead field and computed as a solution of M/EEG forward problem. Thus any measured signal can be modeled as a linear combination of lead fields associated to each dipole source

$$\mathbf{y} = \mathbf{L} \cdot \mathbf{x} + \mathbf{N} \quad (1)$$

where $\mathbf{y} \in \mathbb{R}^n$ is the signal measured by n sensors, \mathbf{L} is the $n \times m$ lead field matrix whose columns represent lead fields of m sources, $\mathbf{x} \in \mathbb{R}^m$ is a vector of sources amplitudes and $\mathbf{N} \in \mathbb{R}^n$ is additive noise. In this work we do not take into account the time component of the signal. The inverse problem aims to find \mathbf{x} knowing \mathbf{y} and \mathbf{L} .

We usually consider all vertices of a cortical mesh as possible source positions which results in $m \gg n$. Thus recovering \mathbf{x} from \mathbf{y} in (1) is an ill-posed problem. In this work, we consider that brain activity which generates an M/EEG signal is a connected cortical region, i.e. there is a path between every pair of vertices. We study the case when only one region is active at once and each dipole in the active region has the same amplitude, i.e. $x_i = a$ if i -th source is inside active region and $x_i = 0$ otherwise.

Numerous methods were proposed to solve this problem [2, 3, 4]. Most source reconstruction methods are based on convex optimization and in consequence identify a single solution. But because of ill-posedness of the problem, it is highly likely that other spatially distinct source configurations can explain the data as well as the identified solution, even under such a strong constraint of being a connected region with constant activity. We propose a method based on agglomerative hierarchical clustering [5], whose objective is not to reconstruct one

active cortical region but to find several ”good” candidates - regions which are different in term of their sizes and/or positions but fit the data with similar accuracy.

2 Clustering algorithm

We define a cluster c_i as a set of vertices of a cortical mesh and denote its size by $|c_i|$. $L(c_i)$ denotes the lead field of a cluster, which, by construction, is a sum of the lead fields of its dipole sources. We initialize our procedure considering each vertex as a cluster. So the vector \mathbf{x} corresponds to the amplitudes of initial clusters. Their initial neighborhood is defined by a cortical mesh. Two vertices are neighbors if they share an edge on the mesh. For any pair of clusters c_i and c_j we define a **potential error**:

$$E(i, j) = \min_a \|y - a(L(c_i) + L(c_j))\|_2 + R(i, j) \quad (2)$$

where y is the M/EEG data to fit, $L(c_i) + L(c_j)$ represents the lead field that we would be obtained by merging the clusters. The first term of the sum represents the data fitting error that would be obtained if the clusters are merged. $R(i, j)$ represents a regularization term which we will discuss in section 2.1. We represent the neighborhood information between clusters as a function $N(i, j) = N(j, i) = 1$, if clusters c_i and c_j are neighbors and 0 otherwise. N is initialized based on the neighborhood of vertices. We denote A as the set of current clusters. Based on this we initialize N and A and proceed with the following steps:

Step 1. Examine all **inter neighbors** potential error (2) and merge the clusters which minimize it:

$$i^*, j^* = \arg \min_{i, j \in A; N(i, j)=1} E(i, j); c_k = c_{i^*} \cup c_{j^*}$$

Step 2. Compute lead field for new cluster: $L(c_k) = L(c_{i^*}) + L(c_{j^*})$

Step 3. Replace two merged clusters by new cluster and update neighborhood information: $A = A \setminus \{c_{i^*}, c_{j^*}\} \cup \{c_k\}$

$$\forall i \in A : N(i, k) = \begin{cases} 1, & \text{if } N(i, i^*) = 1 \text{ or } N(i, j^*) = 1 \\ 0, & \text{otherwise} \end{cases}$$

Step 4. Return to step 1 and repeat until the whole cortex is one cluster.

Merging two clusters can be seen as growing one region in the direction that locally minimizes the regularized data fitting error. Taking into account the neighborhood information guarantees connected regions. The way we compute a lead field for new clusters constrains these regions to have constant activity, i.e. all dipoles of active region have the same amplitude.

In the end, we obtain a dendrogram, which can be cut into a set of spatially separated growing cortical regions (Figure 2). We based the cutting criteria on the "speed" of clusters merging. Let $c_k = c_i \cup c_j$ and $|c_i| \geq |c_j|$. c_i is a cutting point if $|c_j| > s$, where s is arbitrary chosen merging "speed" threshold.

2.1 Regularization

Without regularization ($R(i, j) = 0$) we faced a kind of overfitting problem. The algorithm finds a way not only to reconstruct a region which has a good data fitting error, but also to keep growing the region without significant changes in error (Figure 1a). We believe that it is due to merging dipoles whose lead fields cancel each other out, and by merging "blind" sources - dipoles with a low lead field norm. To solve this problem several regularization approaches can be used: penalize the size of the regions, i.e. do not allow regions to have a big size; introduce a default cortical atlas (e.g. Desikan-Killiany atlas [6]) and allow regions to grow only inside its parcels. In this paper we introduce an approach to regularize regions' isotropy, i.e. to penalize regions with "sharp" borders and holes.

For two clusters c_i and c_j let us define a value $B(i, j)$ as a number of vertices in c_i which have at least one neighbor in c_j . We propose following regularization term:

$$R(i, j) = \lambda \cdot (|c_i| + |c_j|)^2 \cdot \frac{\min(|c_i|, |c_j|)}{B(i, j) + B(j, i)} \quad (3)$$

The ratio term in (3) measures the relative length of the border between clusters c_i and c_j . According to this measure Point 1 in Figure 1b) is more favorable than Point 2 to be merged with the cluster of black points, because it has a longer "merging border". Minimizing this measure favors regions with smooth borders.

The term $\lambda \cdot (|c_i| + |c_j|)^2$ controls the importance of regularization. Being a quadratic function of a cluster size, regularization lets regions grow freely at the beginning and starts to be important for relatively big regions. The hyperparameter λ defines how fast regularization becomes important.

3 Results

We used the "Sample" subject from MNE-python software data set [7] and computed its MEG forward problem. We represented source space as a cortical mesh with about 10000 vertices per hemisphere. Dipole orientations were fixed to be orthogonal to the cortical surface. We simulated one active region with additive noise and applied our reconstruction algorithm. As an output of the algorithm we obtained a set of growing regions and a data fitting error changing with respect to the region size (Figure 1c). With arbitrary chosen error threshold we can select the best regions as well as their lower and upper bound sizes (Figure 1d). As we can see, three spatially separated regions can explain the data with a high accuracy.

4 Conclusion

Our results show that even with a constrained model having only one active region with constant activity, we generally cannot find a unique data-driven solution which is significantly better than others.

The advantage of our method is the concept of spatially separated growing cortical regions. Compared to the methods based

on convex optimization, which return a unique source configuration explaining the data, this concept provides more information about the inverse solution. It provides a relatively small number of candidate regions and estimates their size bounds.

The main directions for future work are to investigate the regularization term and the choice of hyper-parameter; to extend the method for the case when several regions are active at the same time to our clustering approach (for example, adapting MUSIC algorithm [8]) and to perform a multimodal approach (simultaneous EEG and MEG acquisition) to decrease spatial uncertainty of inverse solution.

Acknowledgment: *This work has received funding from the European Research Council (ERC) under the European Union's Horizon 2020 research and innovation program (ERC Advanced Grant agreement No 694665 : CoBCoM - Computational Brain Connectivity Mapping).*

References

- [1] S. Baillet, J. Mosher, R. Leahy, "Electromagnetic brain mapping", IEEE Signal Processing Magazine (2001) 18(6) 14-30
- [2] R. Grech et al. "Review on solving the inverse problem in EEG source analysis", Journal of NeuroEngineering and Rehabilitation 2008, 5:25
- [3] K. Uutela, M. Hämäläinen and E. Somersalo "Visualization of Magnetoencephalographic Data Using Minimum Current Estimates", NeuroImage, **10**, 173–180 (1999)
- [4] Lei Ding, "Reconstructing cortical current density by exploring sparseness in the transform domain", Physics in medicine and biology, **54** (2009) 2683–2697
- [5] F. Murtagh and P. Contreras, "Methods of Hierarchical Clustering", Computing Research Repository - CORR, 2011
- [6] R. Desikan et al., "An automated labeling system for subdividing the human cerebral cortex on MRI scans into gyral based regions of interest", NeuroImage, Volume 31, Issue 3, 1 July 2006, Pages 968-980
- [7] A. Gramfort et al., "MEG and EEG data analysis with MNE-Python", Frontiers in Neuroscience, Volume 7, 2013, ISSN 1662-453X
- [8] N. Mäkelä, M. Stenroos, J. Sarvas and RJ Ilmoniemi, "Truncated RAP-MUSIC (TRAP-MUSIC) for MEG and EEG source localization", NeuroImage, Volume 167, 15 February 2018, Pages 73-83

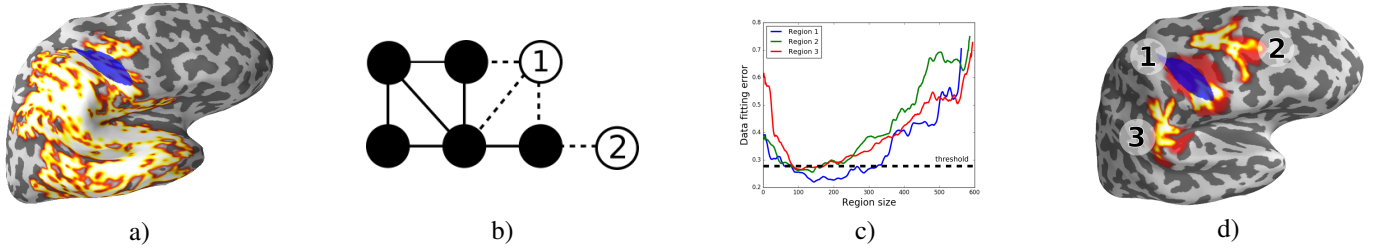


Figure 1: Simulation results: a) simulated region (blue) and reconstructed one (white) without regularization. b) we have two candidates (Point 1 and Point 2) to merge with the cluster of black points. For Point 1 $B(i, j) + B(j, i) = 3 + 1 = 4$ and for Point 2 it is only 2. It results in smaller regularization value (3) for Point 1. Let us notice that merging Point 1 makes the cluster more isotropic compared to Point 2. c) Fitting error as a function of region size for top 3 reconstructed growing regions with isotropy regularization. d) Localization of top 3 regions. Error threshold defines lower and upper bounds of their sizes (yellow and red colors resp.)

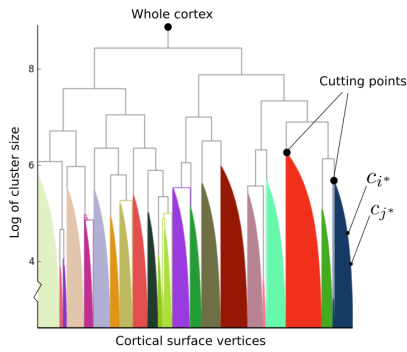


Figure 2: Example of a dendrogram that we get as a result of our clustering algorithm. The y axis represents the logarithm of clusters size for visualization purposes. We can see the particular structure of the tree being a set of smoothly growing sub-trees. Different colors represent extracted growing regions.